

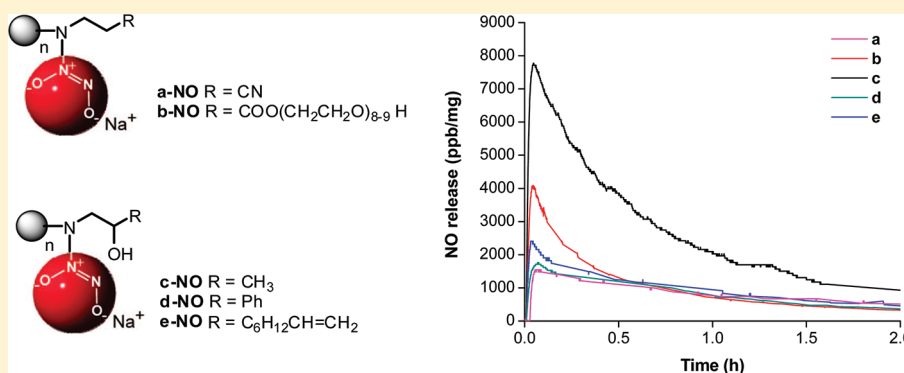
Structurally Diverse Nitric Oxide-Releasing Poly(propylene imine) Dendrimers

Yuan Lu,[†] Bin Sun,[†] Chenghong Li, and Mark H. Schoenfish*

Department of Chemistry, University of North Carolina at Chapel Hill, Chapel Hill, North Carolina 27599, United States

S Supporting Information

ABSTRACT:



Structurally diverse secondary amine-functionalized poly(propylene imine) (PPI) dendrimers capable of tunable nitric oxide (NO) release were synthesized in a straightforward, one-step manner using ring-opening or conjugate-addition reactions with propylene oxide (PO), styrene oxide (SO), acrylonitrile (ACN), poly(ethylene glycol) methyl ether acrylate (average $M_n = 480$) (PEG) or 1,2-epoxy-9-decene (ED). N-Diazeniumdiolate nitric oxide donors were formed on the resulting secondary amine-functionalized G2-G5 PPI dendrimers by reaction with NO gas in basic solution. The NO storage and release kinetics for the resulting dendritic scaffolds were diverse (0.9–3.8 $\mu\text{mol NO/mg}$ totals and 0.3 to 4.9 h half-lives), illustrating the importance of the exterior chemical modification (e.g., steric environments, hydrophobicity, etc.) on diazeniumdiolate stability/decomposition. Tunable NO release was demonstrated by combining two donor systems on the exterior of one macromolecular scaffold. Additionally, a mathematical model was developed that allows for the simulation of dual NO release kinetics using the NO release data from the two single NO donor systems. The approaches described herein extend the range and scope of NO-releasing macromolecular scaffolds by unlocking a series of materials for use as dopants in biomedical polymers or stand-alone therapeutics depending on the exterior modification.

KEYWORDS: dendrimers, nitric oxide, tunable release, diazeniumdiolate

INTRODUCTION

Dendrimers are a family of hyperbranched macromolecules with multivalent surfaces that enable the design of targeted therapeutics agent delivery vehicles.^{1–4} For example, polyamidoamines,⁵ polyamines,⁶ polypeptides,⁷ polyesters,⁸ and polyethers⁹ dendrimers have been utilized for a range of biomedical applications, including drug and gene delivery,^{10–22} biological imaging,^{23–29} and tissue engineering.^{30–33} Bactericidal dendrimers have been prepared by encapsulating antibacterial agents (e.g., sulfamethoxazole³⁴) within the dendrimer or at its periphery (e.g., quaternary ammonium groups³⁵). Anionic amphiphilic dendrimers were also reported to possess antibacterial efficacy against Gram-positive bacteria.³⁶

Nitric oxide is an endogenously produced diatomic free radical that mediates multiple processes in mammalian physiology. Because of NO's pharmacological potential, the synthesis of prodrugs capable of controlled exogenous NO production is important in further understanding NO's role in physiology and

developing NO-based therapeutics. The therapeutic effectiveness of such donors depends on the target (e.g., cell type and condition), concentration and rate of NO release.^{37,38} For example, Chakrapani and co-workers synthesized O2-(2,4-dinitro-5-(4-(N-methylamino)benzoyloxy)phenyl)-1-(N,N-dimethylamino)diazen-1-ium-1,2-diolate (PABA/NO) as an anticancer NO prodrug with efficacy against human leukemia and A2780 human ovarian cancer xenografts.³⁹ Both the NO payload and release kinetics were shown to influence the anticancer activity. The study of how chemical structure impacts the rate of NO release from small molecule NO donors has been an active area of research, particularly with respect to biological activity.^{40–45} Generally, stabilization of the N-diazeniumdiolate NO donor correlates directly with extended NO release.⁴⁶

Received: June 9, 2011

Revised: August 12, 2011

Published: August 29, 2011

To enhance NO storage and release levels relative to small molecule NO donors, we previously reported the synthesis of N-diazeniumdiolate-functionalized poly(propylene imine) (PPI) dendrimer conjugates as macromolecular NO donors capable of storing up to $\sim 5 \mu\text{mol NO/mg}$ with NO release kinetics dependent on the dendrimer structure.⁴⁷ Although we alluded to the multivalent exterior benefit on NO storage/release and further functionalization for imaging, controlled toxicity, and/or active targeting, for example, the study of structure/nitric oxide release relationships was not systematically pursued. In subsequent work, Stasko et al. reported the synthesis of S-nitrosothiol-modified polyamidoamine (PAMAM) dendrimers with alternative decomposition mechanisms for controlled NO release.⁴⁸ Although capable of storing $\sim 2 \mu\text{mol NO/mg}$, the kinetics of NO release were found to be highly dependent on the structure of the nitrosothiol and NO release trigger (e.g., light, copper, temperature). Collectively, the dendritic effects exerted on NO donor stability and reactivity, and the benefits of multifunctionalization with imaging beacons and/or active targeting agents, highlight the tremendous potential of dendrimers as NO release therapeutics.

Herein, we describe the synthesis of N-diazeniumdiolate-functionalized PPI dendrimers using select exterior functionalities to diversify both the NO release kinetics and potential applications for which such materials may prove useful. In addition to assessing the roles of molecular weight (e.g., generation or size of dendrimer) and exterior chemical structure on NO release, we demonstrate the ability to tune NO release kinetics using multiple NO donor functionalization.

EXPERIMENTAL SECTION

Materials and General Considerations. Details of the synthesis of primary amine-functionalized PPI dendrimers (G1 to G5-PPI-NH₂) are provided as Supporting Information. Ethylenediamine (EDA), acrylonitrile (ACN), propylene oxide (PO), styrene oxide (SO), poly(ethylene glycol) methyl ether acrylate (average $M_n = 480$) (PEG), and 1,2-epoxy-9-decene (ED) were purchased from Aldrich Chemical Co. (Milwaukee, WI). 1,6-Hexanediamine (HDA) and sodium methoxide (5.4 M solution in methanol) was purchased from Acros Organics (Geel, Belgium). Sponge cobalt catalyst (A-8B46) was purchased from Johnson Matthey Catalysts (London, U.K.). Common laboratory salts and solvents were purchased from Fisher Scientific (Pittsburgh, PA). All other materials were used as received without further purification unless otherwise noted. ¹H nuclear magnetic resonance (NMR) spectra were recorded on Bruker (400 MHz) and Varian (600 MHz) spectrometers. Hydrogenation reactions used for the synthesis of PPI-NH₂ (e.g., from G2 to G5) were carried out in a stainless steel high-pressure reactor purchased from Parr Instrument Company (Moline, IL). Agitation was provided by a Teflon-coated magnetic stirring bar. Heating was provided using a heating fabric wrapped around the reactor, and temperature was controlled using a temperature controller via a thermal coupler. Nitric oxide release was measured using Sievers 280i Chemiluminesce Nitric Oxide Analyzer (Boulder, CO) as described previously.⁴⁷ The chemiluminescence analyzer was calibrated with NO gas (26.9 ppm). A parameter for converting the instrument response (ppb) to moles of NO was obtained using the conversion of nitrite standards to NO in a 0.1 M KI/H₂SO₄ solution (1.31×10^{-13} moles of NO/ppb).

Synthesis of Secondary Amine-Functionalized PPI Dendrimers. One hundred milligrams of PPI-NH₂ (e.g., from G2 to G5) was dissolved in 2 mL of methanol in a 10 mL vial. One equivalent of acrylonitrile (ACN), poly(ethylene glycol) methyl ether acrylate (average $M_n = 480$) (PEG), propylene oxide (PO), styrene oxide (SO), or 1,2-epoxy-9-decene (ED) (e.g., with respect to molar amount

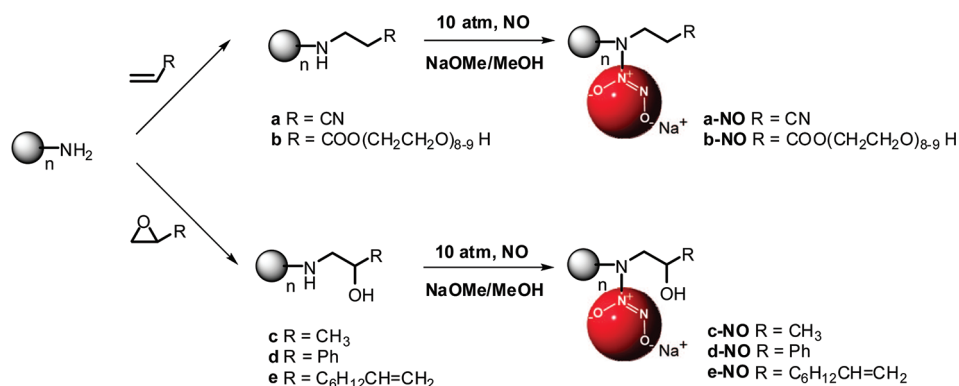
of primary amine functionality) was then added to the 10 mL vial. The solution was stirred at room temperature for 4 days. Solvent was removed under reduced pressure. Dendrimers were dissolved in water followed by dialysis against water and lyophilization.

Representative ¹H NMR data of secondary amine-functionalized G5-PPI conjugate formed via the reactions of G5-PPI-NH₂ with ACN, PEG, PO, SO, and ED (referred to hereafter as G5-PPI-ACN **a-64**, G5-PPI-PEG **b-64**, G5-PPI-PO **c-64**, G5-PPI-SO **d-64**, G5-PPI-ED **e-64**) are as follows. G5-PPI-ACN **a-64**: ¹H NMR (400 MHz, CD₃OD, δ) 2.87 (NHCH₂CH₂CN), 2.82 (NHCH₂CH₂CN), 2.60 (NCH₂CH₂CH₂NH), 2.40 (NCH₂CH₂CH₂NH), 1.60 (NCH₂CH₂CH₂NH). ¹³C NMR (400 MHz, CD₃OD, δ) 117, 52.4, 51.8, 44.5, 33.3, 26.1, 23.6, 16.9. G5-PPI-PEG **b-64**: ¹H NMR (400 MHz, CD₃OD, δ) 2.60 (NCH₂CH₂CH₂NH), 2.40 (NCH₂CH₂CH₂NH), 1.60 (NCH₂CH₂CH₂NH), 3.40–3.70 (OCH₂CH₂O), 2.80 (CH₂NHCH₂CHCOOPEG), 2.65 (CH₂NHCH₂CHCOOPEG), 2.42 (CH₂NHCH₂CHCOOPEG). ¹³C NMR (400 MHz, CD₃OD, δ) 172, 71.6, 70.85, 69.3, 60.1, 57.0, 51.4, 43.9, 39.1, 22.9. G5-PPI-PO **c-64**: ¹H NMR (400 MHz, CD₃OD, δ) 3.70 (CH₂CH(OH)CH₃), 2.60–2.62 (CH₂CH(OH)CH₃, NCH₂CH₂CH₂NH), 2.40 (NCH₂CH₂CH₂NH), 1.60 (NCH₂CH₂CH₂NH), 1.00 (CH₂CH(OH)CH₃). ¹³C NMR (400 MHz, CD₃OD, δ) 66.9, 58.2, 53.7, 52.8, 41.2, 30.8, 27.6, 24.9, 21.8. G5-PPI-SO **d-64**: ¹H NMR (400 MHz, CD₃OD, δ) 7.50–7.20 (CH₂CH(OH)Ph), 3.70 (CH₂CH(OH)Ph), 2.72 (CH₂CH(OH)Ph), 2.60 (NCH₂CH₂CH₂NH), 2.40 (NCH₂CH₂CH₂NH), 1.60 (NCH₂CH₂CH₂NH). ¹³C NMR (400 MHz, CD₃OD, δ) 140.6, 128.2, 127.5, 127.3, 125.8, 71.9, 57.1, 52.4, 45.6, 39.8, 26.3, 23.6. G5-PPI-ED **e-64**: ¹H NMR (400 MHz, CD₃OD, δ) 5.74 (CH₂CH=CH₂), 4.88 (CH₂CH=CH₂), 3.58 (NHCH₂CH(OH)CH₂), 2.60 (NCH₂CH₂CH₂NH), 2.40 (NCH₂CH₂CH₂NH), 1.98 (CH₂CH=CH₂), 1.60 (NCH₂CH₂CH₂NH), 1.2–1.4 ((CH₂)₃CH₂CH=CH₂). ¹³C NMR (400 MHz, CD₃OD, δ) 140.0, 116.1, 70.5, 56.5, 52.4, 47.2, 39.2, 33.9, 30.2, 25.6, 24.9.

Synthesis of Diazeniumdiolate-Functionalized PPI Dendrimers. One equivalent of 5.4 M sodium methoxide solution in methanol (e.g., with respect to the molar amount of primary amine functionalities in PPI-NH₂ used to synthesize these secondary amine-functionalized PPI) was added to a vial containing G2–G5 secondary amine-functionalized PPI dendrimers in methanol (2 mL). The resulting reaction solution was charged with 10 atm of NO while stirring in a stainless steel reactor. Prior to charging with NO, the reactor was flushed three times with argon followed by a series of three longer charge/discharge cycles with argon (3×10 min) to remove oxygen from the stirring solutions. The reactor was then filled with 10 atm of NO (purified over KOH pellets for 30 min to remove trace NO degradation products) at ambient temperature. After 3 days, the NO was expunged using the same charge/discharge procedures described above with argon to remove unreacted NO from the reaction solution.

Characterization of NO Storage and Release. Aliquots (~ 10 – $25 \mu\text{L}$) of diazeniumdiolate-functionalized PPI as a solution in methanol (e.g., ~ 7 – 200 mM) were added to 30 mL deoxygenated phosphate buffered saline (PBS) (10 mM, pH 7.4) at 37 °C to initiate NO release. Nitrogen was flowed through the solution at a flow rate of 70 mL/min to carry the liberated NO to the analyzer. Additional nitrogen flow was supplied to the flask to match the collection rate of the instrument at 200 mL/min. Nitric oxide analysis was terminated when levels decreased to 10 ppb NO/mg dendrimer. Chemiluminescence data for the NO-releasing dendrimers were represented as follows: (i) total amount of NO release ($t[\text{NO}]$, $\mu\text{mol NO/mg}$ and $\mu\text{mol NO}/\mu\text{mol}$ of secondary amine-functionalized dendrimers); (ii) maximum flux of NO release ($[\text{NO}]_{\text{max}}$, ppb/mg of secondary amine-functionalized dendrimers); (iii) half-life ($t_{1/2}$) of NO release; and (iv) conversion efficiency defined as percentages of amine functionalities in PPI (e.g., from G2 to G5) converted to diazeniumdiolate functionality (e.g., total moles of NO release divided by twice the molar amount of primary

Scheme 1. Synthesis of Secondary Amine- and Diazeniumdiolate-Functionalized PPI Conjugates for which n Represents the Number of Primary Amines on the Periphery of PPI Dendrimers ($n = 8, 16, 32, 64$)



amine functionalities in PPI- NH_2 used initially to synthesize secondary amine-functionalized dendrimer conjugates).

RESULTS AND DISCUSSION

Synthesis and Characterization of Secondary Amine-Functionalized PPI Dendrimers. Stasko et al. previously reported an approach whereby secondary amine-functionalized PPI conjugates were reacted with NO at high pressure to form NO-releasing dendritic scaffolds with large NO storage capacity.⁴⁷ Analogously, primary amine-functionalized PPI dendrimers were characterized by significantly less NO storage and shorter NO release durations. These results suggest that the structural features of the dendrimer are critical in the design of diazeniumdiolate-functionalized scaffolds. Since chemical reaction of primary amine functionalities with organic compounds represents a simple approach for designing secondary amine-functionalized PPI conjugates, we targeted the synthesis of secondary amine-functionalized dendrimers using ring-opening and conjugate-addition reactions of PPI- NH_2 with PO, SO, ED, ACN, and PEG (Scheme 1) to fully unlock a series of dendrimer scaffolds with diverse exterior properties (e.g., aromatic, hydrophilic, hydrophobic). Indeed, the epoxides, acrylated and acrylonitrile selected for conjugation were based on sterics, hydrophobicity, and biocompatibility. Of note, it is also possible to yield tertiary amine adducts. In addition, we carried out a series of model kinetic studies using NMR spectroscopy for conjugate-addition reactions of first generation G1-PPI- NH_2 with ACN and ring-opening reactions of HDA with PO to determine the suitability of conjugate-addition and ring-opening reactions for the synthesis of secondary amine-functionalized PPI dendrimers. The results of these studies revealed large differences in the rates of reactions of G1-PPI- NH_2 with ACN, and HDA with PO. The rate constants of the first conjugate-addition or ring-opening reaction (k_1) were substantially larger than those of the second reactions (k_2) (data not shown), providing strong support for the use of such reactions (e.g., over a period of 4 days, in a dilute solution, and at 1 equiv. of ACN, epoxides, or acrylates with respect to molar amount of PPI- NH_2) to yield secondary amine-functionalized products suitable for subsequent NO release studies.

Influence of Exterior Functionality on Nitric Oxide Release. The approach described above is based on dendrimer functionalization at their exterior to yield secondary amine-functionalized PPI dendrimers. Two practical advantages of this approach include that the synthesis is simple and the resulting

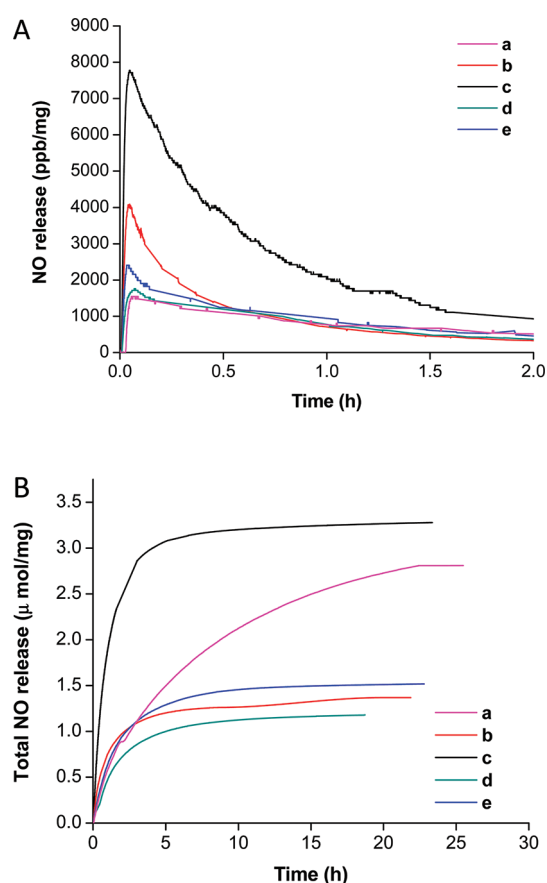


Figure 1. (A) Real time NO release profile for NO-releasing G4-PPI dendrimer conjugates; and (B) plot of $t[\text{NO}]$ vs time for NO-releasing PPI dendrimer conjugates.

structurally diverse exteriors greatly expand the potential applications for which these materials may find utility. Reactions of secondary amine-functionalized PPI (e.g., from G2 to G5) with NO under basic conditions (e.g., sodium methoxide) yielded N-diazeniumdiolate NO donor-functionalized dendrimers with diverse NO release characteristics.

Chemiluminescence was used to characterize the NO storage and release properties (e.g., in PBS, pH 7.4, 37 °C) for the N-diazeniumdiolate-modified PPI dendrimers. Representative NO release profiles for these dendrimers are shown in Figure 1.

Table 1. Nitric Oxide Release Characteristics for PPI Dendrimers in PBS (pH 7.4) at 37 °C

	dendrimer	t[NO] ($\mu\text{mol NO}/\text{mg}$) ^a	t[NO] ($\mu\text{mol NO}/\mu\text{mol}$) ^b	[NO] _{max} (ppb/mg) ^c	[NO] _{max} (ppb/ μmol) ^d	<i>t</i> _{1/2} (h)	conversion (%)
a-8-NO	G2-PPI-ACN-NO	3.57	4.18	1529	1788	4.81	26.1
a-16-NO	G3-PPI-ACN-NO	3.33	8.35	1100	2758	4.84	26.1
a-32-NO	G4-PPI-ACN-NO	2.45	12.7	1547	7977	4.82	19.9
a-64-NO	G5-PPI-ACN-NO	1.68	17.7	881	9282	4.88	13.8
b-8-NO	G2-PPI-PEG-NO	1.11	5.10	3771	17291	0.67	31.9
b-16-NO	G3-PPI-PEG-NO	1.08	10.1	2309	21564	1.11	31.6
b-32-NO	G4-PPI-PEG-NO	1.37	25.8	4088	77035	0.84	40.3
b-64-NO	G5-PPI-PEG-NO	1.17	44.3	1886	71403	1.22	34.6
c-8-NO	G2-PPI-PO-NO	2.99	3.63	17130	20725	0.30	22.7
c-16-NO	G3-PPI-PO-NO	3.22	8.38	9617	24888	0.62	26.2
c-32-NO	G4-PPI-PO-NO	3.27	17.5	7762	41481	0.78	27.3
c-64-NO	G5-PPI-PO-NO	3.78	41.1	6839	74250	1.06	32.1
d-8-NO	G2-PPI-SO-NO	1.14	1.95	8495	14496	1.47	12.2
d-16-NO	G3-PPI-SO-NO	0.91	3.30	2363	8462	0.97	10.3
d-32-NO	G4-PPI-SO-NO	1.18	8.70	1720	12609	1.43	13.6
d-64-NO	G5-PPI-SO-NO	1.25	18.5	2215	32843	1.62	14.5
e-8-NO	G2-PPI-ED-NO	1.95	3.87	5648	11178	0.81	24.2
e-16-NO	G3-PPI-ED-NO	1.64	6.75	2733	11279	1.71	21.1
e-32-NO	G4-PPI-ED-NO	1.51	12.8	2401	20217	1.34	19.9
e-64-NO	G5-PPI-ED-NO	1.86	31.6	3190	54262	1.88	24.7

^a Total amount of NO release (μmol) per milligram of secondary amine-functionalized PPI. ^b Total amount of NO release (μmol) per micromole of secondary amine-functionalized PPI. ^c Maximum flux of NO release (ppb) per milligram of secondary amine-functionalized PPI. ^d Maximum flux of NO release (ppb) per micromole of secondary amine-functionalized PPI.

The workup of specific NO release parameters (e.g., total NO release, maximum flux, half-life, and conversion efficiency) are provided in Table 1. In general, the NO release results reveal high NO storage capabilities (e.g., 0.9–3.8 $\mu\text{mol NO}/\text{mg}$) and a broad range of release kinetics (e.g., NO release half-life from 0.3 to 4.9 h). Further inspection of these data reveals that the conversion efficiencies (e.g., 10–40%) of the dendrimers varied substantially based on the chemical modification. As shown in Table 1, G2 to G5-PPI-SO (**d-NO**) were characterized by lower NO donor formation (e.g., ~10–15%) versus the other PPI dendrimers (e.g., ~14–40%). The lower conversion efficiencies for PPI-SO (**d-NO**) may be attributed to a more sterically hindered environment around the NO donor precursors (i.e., secondary amines), resulting in lower NO and base accessibility to the amines during the NO charging process.

The exterior modification also influenced the NO release kinetics. For example, both PPI-PO (**c-NO**) and PPI-PEG (**b-NO**) released NO rapidly (Table 1 and Figure 1). Such rapid NO release kinetics might be expected since the isopropyl and PEG groups are hydrophilic and facilitate water solvation favorable to diazeniumdiolate NO donor degradation. The data also indicate that the NO release half-lives for G2–G5 PPI-SO (**d-NO**) and PPI-ED (**e-NO**) are slightly longer than PPI-PO (**c-NO**) and PPI-PEG (**b-NO**). The longer NO release for PPI-SO (**d-NO**) and PPI-ED (**e-NO**) correlates well with the increased hydrophobic structure at the exteriors of these dendrimers.

The ACN modification for PPI dendrimer (**a-NO**) exhibited large NO storage (e.g., ~1.7–3.6 $\mu\text{mol NO}/\text{mg}$) and conversion efficiency (e.g., ~14–26%) (Table 1). Of note, past studies have indicated that the reaction of cyano-containing compounds with NO at high-pressures under basic conditions may yield C-diazeniumdiolate-functionalized products. Both NO and nitrous oxide (N_2O) may be release from C-diazeniumdiolates in aqueous

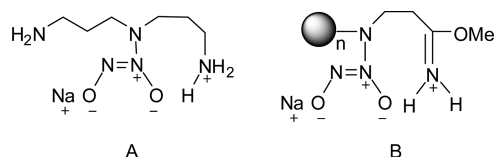


Figure 2. Proposed structures for stabilization of (A) diazeniumdiolate-functionalized DPTA by neighboring cationic ammonium functionality, and (B) PPI-ACN (**a-NO**) by neighboring cationic protonated-imidate functionality.

environments at low pH.^{49–51} In this context, it may be possible that the high conversion efficiencies for PPI-ACN (**a-NO**) arise from the contribution of NO released from C-diazeniumdiolate-functionalized products. A series of experiments were thus carried out to probe the nature of the NO release from PPI-ACN (**a-NO**) using G0.5-PPI, a cyano-containing compound without the capacity to form N-diazeniumdiolate because of the absence of secondary amines. The NO release from G0.5-PPI was $\sim 4.5 \times 10^{-3} \mu\text{mol NO}/\text{mg}$, providing strong support that the high NO storage and conversion efficiency for the ACN-modified dendrimers are indeed the result of N-diazeniumdiolate functionalization.

The PPI-ACN (**a-NO**) analogues were also characterized as having the longest NO release half-lives (e.g., ~5 h). Given the hydrophilic nature of the cyano functionality, the extended NO release is not attributable to water uptake. For example, the long half-lives of N-diazeniumdiolate-functionalized small molecule derivatives (e.g., dipropylenetriamine or DPTA-NO) have previously been attributed to diazeniumdiolate stabilization by neighboring cationic ammonium functionalities as depicted in Figure 2A.^{45,52,53} In this manner, the presence of neighboring cationic functionalities (e.g., protonated imidates) for PPI-ACN (**a-NO**) dendrimers

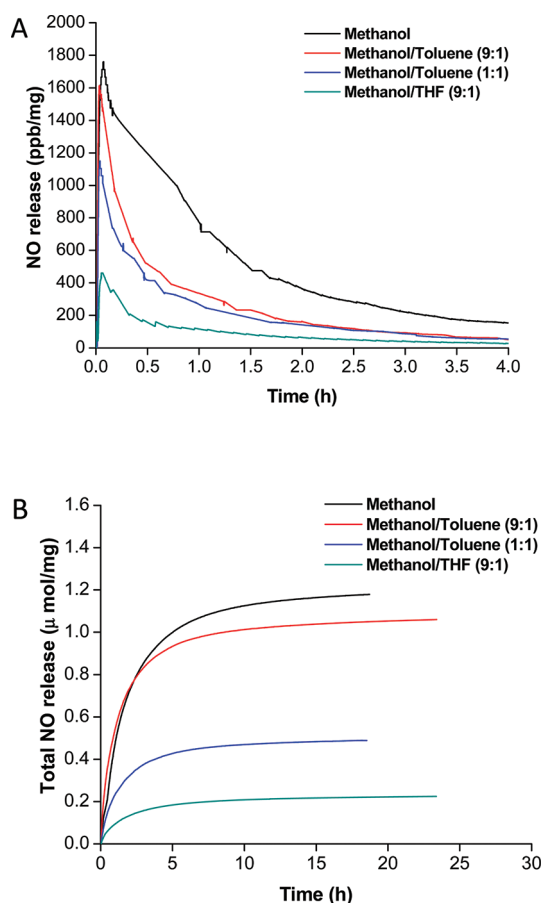


Figure 3. (A) Real time NO release profile and (B) plot of $t[NO]$ vs time for G4-PPI-SO-NO synthesized in different NO conjugation solvents.

may provide additional stabilization to the diazeniumdiolate functionality (Figure 2B).

Since sodium methoxide was used as the base for the reaction of PPI-ACN (**a**) with NO (to yield diazeniumdiolate-functionalized products), the methoxide anion may also serve as a nucleophile to react with the cyano group in PPI-ACN (**a**) and yield imidate adducts.⁵⁴ The transfer of proton from solvent (e.g., methanol) to the relatively basic nitrogen atom in the resulting imidates might thus lead to protonated-imidate functionality (Figure 2B) that is similar to cationic ammonium functionality in DPTA-NO (Figure 2A).

As shown in Table 1, both the NO storage and maximum NO flux per dendrimer molecule increased as a function of dendrimer size (i.e., generation). For example, the NO payload from G5-PPI-PO-NO (**c-64-NO**) was $41.1 \mu\text{mol}/\mu\text{mol}$ dendrimer, much greater than G2-PPI-PO-NO (**c-8-NO**) (e.g., $3.63 \mu\text{mol}/\mu\text{mol}$ dendrimer). A similar trend is observed for maximum NO flux. These results reveal the capability of larger NO-releasing PPI dendrimers to deliver significant concentrations of NO, a potentially beneficial attribute for therapeutic antimicrobial and anticancer applications.

Effect of Solvent for NO Conjugation. As synthesized, the amphiphilic secondary amine-functionalized dendrimers (e.g., PPI-SO, PPI-ED) possess a hydrophilic PPI core and hydrophobic periphery of aromatic rings or long alkyl chains. Different from PPI-ACN, PPI-PO and PPI-PEG, these amphiphilic dendrimers

may have more packed exterior in the charging solvent because of the poor compatibility of the aromatic rings or long alkyl chains with polar solvent (e.g., methanol). We thus sought to investigate the role of charging solvent on NO donor formation efficiency using mixtures of methanol with less polar solvent (e.g., methanol/THF (9:1, v/v), methanol/toluene (9:1, v/v) and methanol/toluene (1:1, v/v)). As shown in Figure 3, the NO release data reveals an adverse effect of toluene and THF on NO conjugation to PPI-SO dendrimers. Compared to toluene, use of THF compromised the NO storage to a larger extent.

The lower NO conjugation efficiency may be the result of the PPI dendrimer core collapsing in the mixture of methanol and less polar solvents (e.g., toluene and THF). Indeed, this hypothesis is supported by dynamic light scattering data (data not shown). In turn, the dendrimer backbone collapse likely contributes to a greater steric hindrance around the secondary amines and concomitant lower NO conjugation efficiency.

Characterization of PPI Conjugates Synthesized from Defined Mixtures of PO and ACN. To evaluate the ability to define NO release, we designed multifunctionalized N-diazeniumdiolate-functionalized dendrimer conjugates using G5-PPI-NH₂ and defined ratios of PO and/or ACN during the functionalization step. Specifically, G5-PPI-NH₂ was reacted with either PO exclusively (e.g., **c-64**), ACN exclusively (e.g., **a-64**), or three different mixtures comprised of PO and ACN at molar ratios of 3:7, 5:5, and 7:3, respectively; the PO, ACN, or defined mixtures of PO and ACN were one equivalent with respect to molar amount of primary amine functionalities in G5-PPI-NH₂. A series of ¹H NMR experiments were carried out on the products of these reactions to determine the actual compositions of PO and ACN conjugated to the G5-PPI-NH₂ (Figure 4). A distinct resonance at 1.10 ppm was apparent corresponding to the methyl protons in the isopropyl group of the products. The chemical shift of this peak was noted in the products for reactions with PO exclusively (e.g., **c-64**) and those with different mixtures of PO and ACN. Further inspection of these data indicates the presence of a second distinct peak at 2.80 ppm, formed upon G5-PPI-NH₂ dendrimer reaction with either ACN exclusively (e.g., **a-64**) or defined mixtures of PO and ACN; this peak corresponds to the methylene protons one carbon away from the cyano group of the products. The compositions of PO and ACN incorporated in the products were 27/73 (**c/a** (27/73)), 40/60 (**c/a** (40/60)), and 60/40 (**c/a** (60/40)), and indicate that the ACN was incorporated at ratios greater than that in the reaction mixtures, likely because of the more rapid reaction of G5-PPI-NH₂ with ACN versus PO.

The NO release from the G5-PPI-PO/ACN conjugates at PO/ACN molar ratios of 27/73, 40/60, and 60/40, respectively, were intermediate to those synthesized based upon G5-PPI-NH₂ reactions with either PO (e.g., **c-64**) or ACN (e.g., **a-64**) alone. Furthermore, the NO release profiles were influenced by the molar ratio of PO/ACN composition. For instance, the NO release was prolonged for the PPI conjugates modified with lower molar ratio of PO/ACN (half-lives of 2.90, 1.57, and 1.10 h for 27/73, 40/60, and 60/40, respectively) (Figure 5A).

A mathematical model was developed to predict the NO release from hybrid G5-PPI-PO/ACN conjugates using the NO release data from the single G5-PPI-PO (**c-64**) and G5-PPI-ACN (**a-64**) systems. In eq 1, $a:b$ is the molar ratio of the PO and ACN modification in the hybrid G5-PPI-PO/ACN conjugate as determined by NMR spectroscopy, whereas y_{PO} and y_{ACN} represent the normalized NO release profiles of the G5-PPI-PO

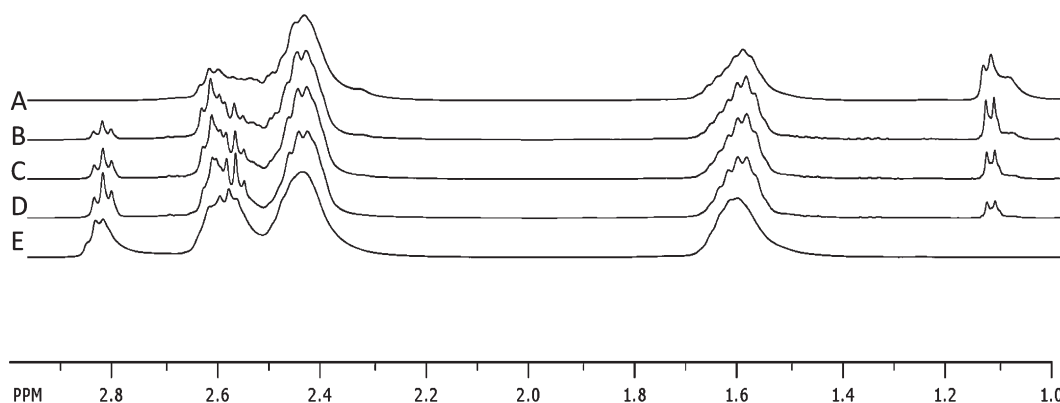


Figure 4. ^1H NMR spectra of (A) G5-PPI-PO (c-64), (E) G5-PPI-ACN (a-64), and G5-PPI-PO/ACN at molar ratios of (B) 7:3, (C) 5:5, and (D) 3:7. The actual compositions of PO and ACN incorporated into these three PPI conjugates are at molar ratios of (B) 27/73, (C) 40/60, and (D) 60/40, respectively, as determined by integrating two chemical shifts at 1.10 and 2.80 ppm.

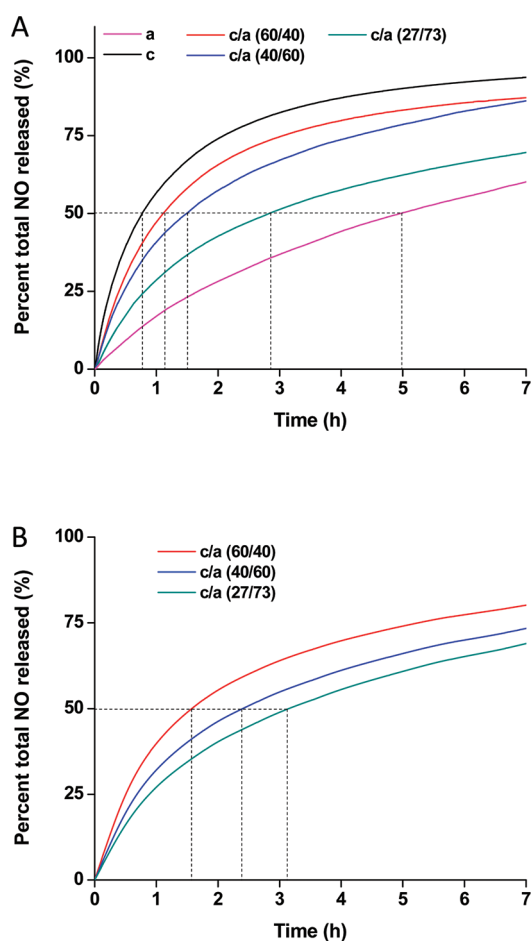


Figure 5. (A) Experimental plot of percent total NO released in PBS (pH 7.4) at 37 °C as a function of time for G5-PPI-PO (c-NO), G5-PPI-ACN (a-NO), and G5-PPI-PO/ACN conjugates; (B) simulated plot of percent total NO released for G5-PPI-PO/ACN conjugates.

(c-64) and G5-PPI-ACN (a-64) systems, respectively. Simulated NO release from a hybrid G5-PPI-PO/ACN conjugate ($y_{a:b}$) was thus derived by averaging the normalized NO release from G5-PPI-PO (c-64) (y_{PO}) and G5-PPI-ACN (a-64) (y_{ACN}) weighted with respect to the mole percentages of PO (i.e., $[a/(a+b)] \times 100\%$)

and ACN (i.e., $[b/(a+b)] \times 100\%$) modification in the hybrid G5-PPI-PO/ACN conjugate.

$$y_{a:b} = y_{\text{PO}} \frac{a}{a+b} + y_{\text{ACN}} \frac{b}{a+b} \quad (1)$$

As shown in Figure 5B, the simulated NO release from G5-PPI-PO/ACN conjugates were comparable with the experimental data, even though the experimental hybrid PPI conjugates were characterized by slightly faster NO release (e.g., the simulated NO release half-lives of 3.13, 2.42, and 1.65 h for c/a (27/73), c/a (40/60), and c/a (60/40), respectively). Nevertheless, the developed mathematical model appears to be well suited for simulating dual NO release kinetics using NO release data from single NO donor systems. For dendrimers, these results demonstrate that functionalization of PPI- NH_2 with a defined mixture of PO and ACN allows for precise NO release selection with access to NO release kinetics that are intermediate to those formed upon reactions with one NO donor type exclusively.

CONCLUSIONS

To expand the utility of macromolecular NO-release scaffolds as stand-alone therapeutics, dopants for biomedical polymers, or general NO-release sources, we synthesized a series of diverse NO-releasing PPI dendrimers by straightforward chemical modification of the core dendrimer using conjugation addition (ACN and PEG) or ring-opening (PO, ED, and SO) reactions. The NO release from these resulting dendrimers demonstrated that size (i.e., generation number or molecular weight) and exterior structures (e.g., steric environment, hydrophobicity, etc.) play important roles in NO release kinetics. Furthermore, the use of select NO donors with unique NO release kinetics and overall payloads may be exploited by multi-NO donor/dendrimer functionalization. The combination of structural diversity and achievable NO release (i.e., up to 3.8 μmol NO/mg with half-lives from 0.3 to 4.9 h) should prove useful in the further study and utilization of these NO release materials for a broad range of fundamental and applied applications including pharmacological agents.

ASSOCIATED CONTENT

S Supporting Information. Details of the synthesis of primary amine-functionalized PPI conjugates from first to fifth

generation. This material is available free of charge via Internet at <http://pubs.acs.org>.

AUTHOR INFORMATION

Corresponding Author

*E-mail: schoenfisch@unc.edu.

Author Contributions

[†]These authors contributed equally to this work.

ACKNOWLEDGMENT

Financial support was provided by the National Institutes of Health (NIH EB000708). We are grateful to Professor Michel Gagne and Mr. Harlan Mangum at the University of North Carolina at Chapel Hill for providing and assisting in the use of the high-pressure reactor. We also thank Dr. Marc ter Horst for technical assistance and helpful discussion involving ¹H NMR analysis of the dendrimers.

REFERENCES

- (1) Lee, C. C.; MacKay, J. A.; Frechet, J. M. J.; Szoka, F. C. *Nat. Biotechnol.* **2005**, *23*, 1517–1526.
- (2) Mintzer, M. A.; Grinstaff, M. W. *Chem. Soc. Rev.* **2011**, *40*, 173–190.
- (3) Wolinsky, J. B.; Grinstaff, M. W. *Adv. Drug Delivery Rev.* **2008**, *60*, 1037–1055.
- (4) Joshi, N.; Grinstaff, M. *Curr. Top. Med. Chem.* **2008**, *8*, 1225–1236.
- (5) Tomalia, D. A.; Naylor, A. M.; Goddard, W. A. *Angew. Chem., Int. Ed.* **1990**, *29*, 138–175.
- (6) Debrabandervandenbergh, E. M. M.; Meijer, E. W. *Angew. Chem., Int. Ed.* **1993**, *32*, 1308–1311.
- (7) Sadler, K.; Tam, J. P. *Rev. Mol. Biotechnol.* **2002**, *90*, 195–229.
- (8) Ihre, H.; Hult, A.; Soderlind, E. *J. Am. Chem. Soc.* **1996**, *118*, 6388–6395.
- (9) Hawker, C. J.; Frechet, J. M. J. *J. Am. Chem. Soc.* **1990**, *112*, 7638–7647.
- (10) Allen, T. M.; Cullis, P. R. *Science* **2004**, *303*, 1818–1822.
- (11) Malik, N.; Evagorou, E. G.; Duncan, R. *Anti-Cancer Drugs* **1999**, *10*, 767–776.
- (12) Matsumura, Y.; Maeda, H. *Cancer Res.* **1986**, *46*, 6387–6392.
- (13) Kukowska-Latallo, J. F.; Candido, K. A.; Cao, Z. Y.; Nigavekar, S. S.; Majoros, I. J.; Thomas, T. P.; Balogh, L. P.; Khan, M. K.; Baker, J. R. *Cancer Res.* **2005**, *65*, 5317–5324.
- (14) Wooley, K. L.; Hawker, C. J.; Frechet, J. M. J. *J. Am. Chem. Soc.* **1993**, *115*, 11496–11505.
- (15) Gillies, E. R.; Frechet, J. M. J. *J. Am. Chem. Soc.* **2002**, *124*, 14137–14146.
- (16) Steffensen, M. B.; Simanek, E. E. *Angew. Chem., Int. Ed.* **2004**, *43*, 5178–5180.
- (17) Li, Y. G.; Cu, Y. T. H.; Luo, D. *Nat. Biotechnol.* **2005**, *23*, 885–889.
- (18) Haensler, J.; Szoka, F. C. *Bioconjugate Chem.* **1993**, *4*, 372–379.
- (19) Tang, M. X.; Redemann, C. T.; Szoka, F. C. *Bioconjugate Chem.* **1996**, *7*, 703–714.
- (20) Vincent, L.; Varet, J.; Pille, J. Y.; Bompais, H.; Opolon, P.; Maksimenko, A.; Malvy, C.; Mirshahi, M.; Lu, H.; Soria, J. P. V. C.; Li, H. *Int. J. Cancer* **2003**, *105*, 419–429.
- (21) Thomas, T. P.; Shukla, R.; Kotlyar, A.; Kukowska-Latallo, J.; Baker, J. R. *Bioorg. Med. Chem. Lett.* **2010**, *20*, 700–703.
- (22) Majoros, I. J.; Myc, A.; Thomas, T.; Mehta, C. B.; Baker, J. R. *Biomacromolecules* **2006**, *7*, 572–579.
- (23) Wiener, E. C.; Brechbiel, M. W.; Brothers, H.; Magin, R. L.; Gansow, O. A.; Tomalia, D. A.; Lauterbur, P. C. *Magnet. Reson. Med.* **1994**, *31*, 1–8.
- (24) Margerum, L. D.; Campion, B. K.; Koo, M.; Shargill, N.; Lai, J. J.; Marumoto, A.; Sontum, P. C. *J. Alloys Compd.* **1997**, *249*, 185–190.
- (25) Kobayashi, H.; Kawamoto, S.; Choyke, P. L.; Sato, N.; Knopp, M. V.; Star, R. A.; Waldmann, T. A.; Tagaya, Y.; Brechbiel, M. W. *Magn. Reson. Med.* **2003**, *50*, 758–766.
- (26) Ziemer, L. S.; Lee, W. M. F.; Vinogradov, S. A.; Sehgal, C.; Wilson, D. F. *J. Appl. Physiol.* **2005**, *98*, 1503–1510.
- (27) Dunphy, I.; Vinogradov, S. A.; Wilson, D. F. *Anal. Biochem.* **2002**, *310*, 191–198.
- (28) Brinas, R. P.; Troxler, T.; Hochstrasser, R. M.; Vinogradov, S. A. *J. Am. Chem. Soc.* **2005**, *127*, 11851–11862.
- (29) Floyd, W. C.; Klemm, P. J.; Smiles, D. E.; Kohlgruber, A. C.; Pierre, V. C.; Mynar, J. L.; Frechet, J. M. J.; Raymond, K. N. *J. Am. Chem. Soc.* **2011**, *133*, 2390–2393.
- (30) Rozhkov, V.; Wilson, D.; Vinogradov, S. *Macromolecules* **2002**, *35*, 1991–1993.
- (31) Cloninger, M. J. *Curr. Opin. Chem. Biol.* **2002**, *6*, 742–748.
- (32) Wathier, M.; Jung, P. J.; Camahan, M. A.; Kim, T.; Grinstaff, M. W. *J. Am. Chem. Soc.* **2004**, *126*, 12744–12745.
- (33) Velazquez, A. J.; Carnahan, M. A.; Kristinsson, J.; Stinnett, S.; Grinstaff, M. W.; Kim, T. *Arch. Ophthalmol.-Chic.* **2004**, *122*, 867–870.
- (34) Ma, M. L.; Cheng, Y. Y.; Xu, Z. H.; Xu, P.; Qu, H.; Fang, Y. J.; Xu, T. W.; Wen, L. P. *Eur. J. Med. Chem.* **2007**, *42*, 93–98.
- (35) Chen, C. Z. S.; Beck-Tan, N. C.; Dhurjati, P.; van Dyk, T. K.; LaRossa, R. A.; Cooper, S. L. *Biomacromolecules* **2000**, *1*, 473–480.
- (36) Meyers, S. R.; Juhn, F. S.; Griset, A. P.; Luman, N. R.; Grinstaff, M. W. *J. Am. Chem. Soc.* **2008**, *130*, 14444–14445.
- (37) Hofseth, L. J.; Hussain, S. P.; Wogan, G. N.; Harris, C. C. *Free Radical Bio. Med.* **2003**, *34*, 955–968.
- (38) Pacher, P.; Beckman, J. S.; Liaudet, L. *Physiol. Rev.* **2007**, *87*, 315–424.
- (39) Chakrapani, H.; Wilde, T. C.; Citro, M. L.; Goodblatt, M. M.; Keefer, L. K.; Saavedra, J. E. *Bioorg. Med. Chem.* **2008**, *16*, 2657–2664.
- (40) Velazquez, C. A.; Chen, Q. H.; Citro, M. L.; Keefer, L. K.; Knaus, E. E. *J. Med. Chem.* **2008**, *51*, 1954–1961.
- (41) Chakrapani, H.; Showalter, B. M.; Kong, L.; Keefer, L. K.; Saavedra, J. E. *Org. Lett.* **2007**, *9*, 3409–3412.
- (42) Velazquez, C. A.; Rao, P. N. P.; Citro, M. L.; Keefer, L. K.; Knaus, E. E. *Bioorg. Med. Chem.* **2007**, *15*, 4767–4774.
- (43) Keefer, L. K.; Flippin-Anderson, J. L.; George, C.; Shanklin, A. P.; Dunams, T. A.; Christodoulou, D.; Saavedra, J. E.; Sagan, E. S.; Bohle, D. S. *Nitric Oxide-Biol. Chem.* **2001**, *5*, 377–394.
- (44) Davies, K. M.; Wink, D. A.; Saavedra, J. E.; Keefer, L. K. *J. Am. Chem. Soc.* **2001**, *123*, 5473–5481.
- (45) Keefer, L. K.; Nims, R. W.; Davies, K. M.; Wink, D. A. *Method Enzymol.* **1996**, *268*, 281–293.
- (46) Hrabie, J. A.; Klose, J. R.; Wink, D. A.; Keefer, L. K. *J. Org. Chem.* **1993**, *58*, 1472–1476.
- (47) Stasko, N. A.; Schoenfisch, M. H. *J. Am. Chem. Soc.* **2006**, *128*, 8265–8271.
- (48) Stasko, N. A.; Fischer, T. H.; Schoenfisch, M. H. *Biomacromolecules* **2008**, *9*, 834–841.
- (49) DeRosa, F.; Kibbe, M. R.; Najjar, S. F.; Citro, M. L.; Keefer, L. K.; Hrabie, J. A. *J. Am. Chem. Soc.* **2007**, *129*, 3786–3787.
- (50) Arnold, E. V.; Citro, M. L.; Keefer, L. K.; Hrabie, J. A. *Org. Lett.* **2002**, *4*, 1323–1325.
- (51) Arnold, E. V.; Keefer, L. K.; Hrabie, J. A. *Tetrahedron Lett.* **2000**, *41*, 8421–8424.
- (52) Shin, J. H.; Schoenfisch, M. H. *Chem. Mater.* **2008**, *20*, 239–249.
- (53) Kim, J.; Lee, Y.; Singha, K.; Kim, H. Y.; Shin, J. H.; Jo, S.; Han, D. K.; Kim, W. J. *Bioconjugate Chem.* **2011**, *22*, 1031–1038.
- (54) Schaefer, F. C.; Peters, G. A. *J. Org. Chem.* **1961**, *26*, 412–418.